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(54) **Polymer film for wrapping a stent structure**

Polymerfilm zum Umhüllen einer Stentstruktur

Film polymère pour envelopper un stent

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Description

BACKGROUND OF THE INVENTION

Field of the Invention

[0001] This invention relates generally to expandable intraluminal vascular grafts, generally referred to as stents, and more particularly concerns metal stents wrapped with a polymer film capable of carrying and releasing therapeutic drugs.

Description of Related Art

[0002] Stents typically are implanted within a vessel in a contracted state and then expanded when in place in the vessel in order to maintain patency of the vessel to allow fluid flow through the vessel. Ideally, implantation of such stents is accomplished by mounting the stent on the balloon portion of a catheter, positioning the stent in a body lumen, and expanding the stent to an expanded state by inflation of a balloon within the stent. The stent then can be left in place by deflating the balloon and removing the catheter.

[0003] Stents commonly have a metallic structure to provide the strength required to function as a stent, but typically do not provide for the delivery of localized therapeutic pharmacological treatment of a vessel at the location being treated with the stent. Polymeric materials capable of absorbing and releasing therapeutic agents may not fulfill the structural and mechanical requirements of a stent, especially when the polymeric materials are loaded with a drug, because drug-loading of a polymeric material can significantly affect the structural and mechanical properties of the polymeric material. Because it often is useful to provide localized therapeutic pharmacological treatment of a vessel at the location being treated with the stent, it would be desirable to combine such polymeric materials with existing stent structures to provide a stent with the capability of absorbing therapeutic drugs or other agents, for placement and release of the therapeutic agents at a specific intravascular site.

[0004] In WO-A-95/29647 there is described a metal stent for vascular implantation having a covering sleeve of collagen material. The stent is of the variable diameter type, and the sleeve may be stretched into place or otherwise positioned between the stent and the vascular wall when the stent is seated or deployed. A drug or other agent such as heparin or the like may be included in the collagen for release after stent deployment.

[0005] EP-A-0,578,998 describes an endoprosthesis formed as an elongated hollow body for implantation in a blood vessel or other body cavity by means of a catheter. It has a coating made of polyactide or of albumin bound with glutaraldehyde capable of imparting a medical preparation to a patient once implanted at an even rate continuously. The coating completely encloses all

parts of the endoprosthesis.

SUMMARY OF THE INVENTION

5 [0006] According to the present invention there is provided a drug-loaded stent, comprising: an expandable stent structural member; and a polymeric material disposed on the stent structural member, the polymeric material being loaded with a therapeutic agent, character-
10 ised in that the polymeric material is a planar sheet wrapped in a coil around the stent structural member

[0007] Thus the present invention provides a stent wrapped with a polymer film capable of carrying and releasing therapeutic agents. Because the polymer film is preferably wrapped on the outside of the stent, and is not needed to provide structural strength to assist in opening the flow path of the vasculature or other body lumen where the stent is to be placed, the drug-containing section can be specially formulated for its specific
15 function of delivering drugs locally. The stent can be used in coronary arteries or any other part of the vasculature or other body lumen where mechanical opening force is necessary or desirable to keep the vessel open or to maintain the stent flush against the lumen wall, and where an anti-restenosis, anti-proliferative or other type
20 of therapeutic drug or agent simultaneously is to be positioned and diffused.

[0008] Particular embodiments accordingly provide — a drug-loaded stent, comprising an expandable stent structural member, and a planar sheet of polymeric material disposed on the outside of the expandable stent structural member. The polymeric material preferably is bioabsorbable, and preferably is loaded or coated or laminated with a therapeutic agent or drug to reduce or prevent restenosis and thrombosis in the vessel being
25 treated. The polymer material can be a thermoplastic or an elastomer, for example, so that the film can stretch or deform radially when the stent structural member is expanded. The film of polymer material can be formed
30 as a solid sheet, or can incorporate holes of various sizes and shapes to promote rapid endothelialization.

[0009] The polymer film preferably is mounted to the stent structural member, and in a presently preferred embodiment, the polymer film can be attached to the existing stent structural member in an unexpanded state by adhesive or by heat sealing, with the stent structural member sandwiched between internal and external layers of film heat sealed around the stent structural member, or mechanically, as by such a mechanical connection as hooking one or more slots on an edge portion of the polymeric material through a corresponding slotted portion of the stent structural member, or with a metal clip. The polymer material can be attached to the stent structural member at one or more points, and wrapped
35 so that the diameter of the outer coiled film would uncoil and expand in diameter to match the diameter of the metal stent. When coiled around the stent structural member, the coiled polymer film can have at least one

slit transverse to the longitudinal axis about which the stent is coiled to accommodate possible uneven expansion of the underlying stent structural member.

[0010] In another presently preferred embodiment, the polymer material can be attached to an existing stent structural member with an interference fit by tightly wrapping the polymer film at least once circumferentially around the stent structural member in an unexpanded state and attaching the polymer film to itself to form a sleeve around the stent structural member, such as by heating and melting the film to itself, adhesive bonding, solvent bonding, bonding one or more strips of elastic polymeric material on the outside edge of the polymeric film wrap to secure it, or by mechanical fastening, such as by a clip.

[0011] In one currently preferred embodiment, the polymer material can be attached to an existing stent structural member by hooking one or more slots on an edge portion of the polymeric material through a corresponding slotted portion of the stent structural member, tightly wrapping the polymer film at least once circumferentially around the stent structural member in an unexpanded state to form a coil of layers of the polymeric material, and securing the layers in a tightly wrapped coil. The coil currently is preferably secured in a tightly wrapped coil by adhesive bonding, typically by an adhesive such as a copolymer of poly-L-lactic acid (L-PLA) and polycaprolactone (PCL), although other adhesives, heat bonding, solvent bonding, or one or more mechanical fasteners, such as with a metal clip, for example, also may be suitable. Alternatively, the coil can be secured in a tightly wrapped coil by attaching one end of at least one piece of elastic material to an exterior end portion of the coil of polymeric material, and attaching the other end of the elastic material to a portion of the exterior of the wrapped coil of polymeric material. The elastic material stretches to allow the coil of polymeric material to uncoil as the stent is expanded.

[0012] In another currently preferred embodiment, a combination of a stent structural member and a polymeric film wrapping can be provided with a coating of lubricious material. The lubricious material currently preferably comprises a mixture of polyethylene oxide and polyethylene glycol, although other types of hydrophilic polymeric materials such as polyethylene acetate, polyvinyl pyrrolidone (PVP), polyvinyl alcohol, polyacrylamide, hydrophilic soft segment urethanes, soem natural gums such as gum arabic, gum tragacanth and the like, polyanhydrides or other similar hydrophilic polymers, and combinations thereof, also can be used. The lubricious coating currently preferably is applied over a stent-and-polymer-film-wrap combination by dipping the wrapped stent in the hydrated, liquid lubricious material. The layer of lubricious material protects the stent from the guide catheter or the body lumen in which the stent is inserted by providing a low friction surface over the stent.

[0013] These and other aspects and advantages of

the invention will become apparent from the following detailed description, and the accompanying drawings, which illustrate by way of example the features of the invention.

BRIEF DESCRIPTION OF THE DRAWINGS

[0014]

FIGURE 1 is a cross-sectional view of a first embodiment of the stent structural member and film of polymer material of the drug-loaded stent of the invention shown in an unexpanded state;

FIG. 2 is a cross-sectional view of the drug-loaded stent of FIG. 1 shown in an expanded state;

FIG. 3 is a perspective view of the drug-loaded stent of FIG. 1;

FIG. 4 is a perspective view of an alternate embodiment of the drug-loaded stent of FIG. 1 having apertures in the exterior sheet of polymeric material;

FIG. 5 is a cross-sectional view of a second embodiment of the drug-loaded stent of the invention, shown in an unexpanded state;

FIG. 6 is a perspective view of an alternate embodiment of the drug-loaded stent of FIG. 5 having apertures in the polymeric material;

FIG. 7 is a cross-sectional view of an alternate embodiment of the drug-loaded stent of FIG. 5 having multiple wrappings of the polymeric material;

FIG. 8 is an elevational view of a representative stent structural member, shown in a vessel;

FIG. 9 is a plan view of a sheet of polymeric material in another alternative embodiment including elastic strips for securing the polymeric material wrapped around a stent structural member;

FIG. 10 is a cross-sectional view of a drug-loaded stent wrapped with the polymeric material of FIG. 9;

FIG. 11 is a perspective view of the drug-loaded stent of FIG. 10;

FIG. 12 is a plan view of a sheet of polymeric material in a further alternative embodiment including an elastic strip extending the width of the polymeric material for securing the polymeric material when wrapped around a stent structural member;

FIG. 13 is a perspective view of a drug-loaded stent wrapped with the polymeric material of FIG. 12;

FIG. 14 is a plan view of a sheet of polymeric material in a further alternative embodiment including attachment tabs for securing the polymeric material to a stent structural member;

FIG. 15 is an elevational view of a drug-loaded stent wrapped with the sheet of polymeric material of FIG. 14 and mounted on a balloon dilatation catheter for delivery;

FIG. 16 is an enlarged partial sectional view of the drug-loaded stent of FIG. 15 showing the sheet of polymeric material wrapped around a slotted tube stent structural member;

FIG. 17 is an elevational view of the drug-loaded stent of FIG. 15 covered with a layer of a lubricious, hydrophilic polymeric coating; and

FIG. 18 is a partial sectional view of the drug-loaded stent of FIG. 17.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

[0015] Stents that have a metallic structure typically do not provide for the delivery of localized therapeutic drugs in a blood vessel, while polymeric materials that can be used for drug delivery may not fulfill the structural and mechanical requirements of a stent to hold open a body lumen. Polymeric materials used for the dual function of structural support and for absorbing and releasing therapeutic agents may not fulfill either function satisfactorily, because drug-loading of a polymeric material can significantly affect the structural and mechanical properties of the polymeric material, and the ability to absorb and release therapeutic agents or drugs can affect structural characteristics.

[0016] Accordingly, as shown in FIGS. 1-4, one embodiment of the present invention provides for a stent 20 that can be drug-loaded, comprising an expandable stent structural member 22, and a planar sheet or film 24 of polymeric material, further described below, that in a first embodiment is attached to the metal stent at one or more points of attachment 26, and is wrapped in a coil around the stent in an unexpanded state. The polymer material can be extruded as a thin film, and any processing can be done while the material is in a flat sheet form.

[0017] The attachment of the film of polymeric material 24 to the stent structural member 22 in an unexpanded state can be by adhesive; heat sealing such as with the stent structural member sandwiched between internal and external layers of film heat-sealed or otherwise laminated around the stent structural member; by mechanical connection such as by hooking one or more slots on an edge portion of the polymeric material through a corresponding slotted portion of the stent

structural member, as will be described further below, or with a metal clip, for example. The film of polymeric material also has a free end 28, and can have one or more slits 30 in the polymeric film transverse to the axis 32 of the stent to accommodate possible uneven expansion of the underlying stent structural member. The planar sheet of polymeric material preferably is adapted to uncoil and to expand to match the expansion of the stent structural member. The planar sheet of polymeric material can be a solid sheet, or can have a surface defining a plurality of apertures 34 of various sizes and shapes to promote rapid endothelialization, as is illustrated in FIG. 4. The stent can be mounted on a balloon dilatation catheter, for deployment of the stent in the vasculature of a patient.

[0018] As is illustrated in FIG. 5, in a second embodiment of the stent 40 that can be drug-loaded, the stent comprises a stent metal structural member 42, and a planar sheet or film of polymeric material 44, further described below. The film of polymeric material in this embodiment has a first end 46 forming a first layer 47 of the polymeric material, and a second end 48 overlapping the first end forming a second layer 49 and attached to the first layer of the polymeric film, preferably by heating and melting the film to itself to form a longitudinal heat seal bond 50 between the first and second layers. Attachment of the two outer layers of the polymeric film also can be accomplished by adhesive bonding, solvent bonding, or one or more mechanical fasteners, such as with a metal clip, for example. In this embodiment, the planar sheet of polymeric material preferably is wrapped circumferentially and cinched tightly as a sleeve around the stent structural member, and thus is attached to the stent structural member by an interference fit. In an alternative embodiment illustrated in FIG. 7, the polymeric material can be wrapped multiple times around the stent to form multiple layers that can be joined together as described with reference to FIG. 5 to form a tube around the stent.

[0019] The primary function of the sheet of polymeric material is to deliver therapeutic agents or drugs to help prevent thrombosis and/or restenosis. The planar sheet of polymeric material preferably is selected from the group of polymers consisting of thermoplastic and elastomeric polymers, so that the polymeric film can stretch or deform radially when the stent structural member is expanded.

[0020] As is shown in FIG. 6, the planar sheet of polymeric material also can have a surface defining a plurality of apertures 52 of various sizes and shapes to promote rapid endothelialization, similar to the embodiment illustrated in FIG. 4. The stent can be mounted on a balloon dilatation catheter, for deployment of the stent in the vasculature of a patient.

[0021] In each of these embodiments, the stent structural member is of the type that can be implanted within a vessel in a contracted state and expanded to maintain patency of the vessel and to allow fluid flow through the

vessel, such as the expanding stents available from Advanced Cardiovascular Systems, Inc., Santa Clara, CA (ACS), the Johnson & Johnson Corporation (e.g., Palmaz-Shatz stents) Cook Incorporated (e.g., Gianturco stents), and the like. The metal structural member, for example, can be formed from a metal selected from the group of metals consisting of stainless steel, MP35N, MP20N, elastin (nitinol), tantalum, nickel-titanium alloy, platinum-iridium alloy, gold, and magnesium, although the stent structural member also can be formed of suitable non-metallic materials. "MP35N" and "MP20N" are trade names for alloys of cobalt, nickel, chromium and molybdenum that are available from Standard Pressed Steel Co. of Jenkintown, Pennsylvania. MP35N consists of 35% cobalt, 35% nickel, 20% nickel, 20% chromium, and 10% molybdenum.

[0022] A representative stent structural member 60 with which a sheet of polymeric material can be combined is illustrated in FIG. 8. In one preferred embodiment, the stent structural member 60 can be formed of metal, and comprises a plurality of radially expandable cylindrical elements 62 disposed coaxially and interconnected by members 63 disposed between adjacent cylindrical elements. The stent structural member is shown without a covering sheet of polymeric material, in a typical setting within a vessel 65, for repairing a detached vessel lining 66, for example, and for maintaining the patency of the vessel.

[0023] The polymeric material preferably is selected from thermoplastic and elastomeric polymers. In one currently preferred embodiment, the polymeric material can be a material available under the trade name "C-Flex" from Concept Polymer Technologies of Largo, Florida. In another currently preferred embodiment, the polymeric material can be ethylene vinyl acetate (EVA); and in yet another currently preferred embodiment, the polymeric material can be a material available under the trade name "BIOSPAN." Other suitable polymeric materials include latexes, urethanes, polysiloxanes, and modified styrene-ethylene/butylene-styrene block copolymers (SEBS) and their associated families, as well as elastomeric, bioabsorbable, linear aliphatic polyesters. The polymeric material typically can have a thickness in the range of about 0.051 to 0.508 millimeters (about 0.002 to about 0.020 inches), for example. The polymeric material preferably is bioabsorbable, and is preferably loaded or coated with a therapeutic agent or drug, including, but not limited to, antiplatelets, antithrombins, cytostatic and antiproliferative agents, for example, to reduce or prevent restenosis in the vessel being treated. The therapeutic agent or drug preferably is selected from the group of therapeutic agents or drugs consisting of sodium heparin, low molecular weight heparin, hirudin, argatroban, forskolin, vapiprost, prostacyclin and prostacyclin analogues, dextran, D-phenylpropane-arg-chloromethylketone, dipyridamole, glycoprotein IIb/IIIa platelet membrane receptor antibody, recombinant hirudin, thrombin inhibitor, angiopeptin, an-

giotensin converting enzyme inhibitors, (such as Captopril, available from the Squibb Corporation; Cilazapril, available from the Hoffman-La Roche Company; or Lisinopril, available from the Merck Company) calcium channel blockers, colchicine, fibroblast growth factor antagonists, fish oil, omega 3-fatty acid, histamine antagonists, HMG-CoA reductase inhibitor, methotrexate, monoclonal antibodies, nitroprusside, phosphodiesterase inhibitors, prostaglandin inhibitor, seramin, serotonin blockers, steroids, thioprotease inhibitors, triazopyrimidine and other PDGF antagonists, alpha-interferon and genetically engineered epithelial cells, and combinations thereof. While the foregoing therapeutic agents have been used to prevent or treat restenosis and thrombosis, they are provided by way of example and are not meant to be limiting, as other therapeutic drugs may be developed which equally are applicable for use with the present invention.

[0024] In another currently preferred embodiment illustrated in FIGS. 9-13, the stent 70 that can be drug-loaded comprises a stent metal structural member 72, such as the stent structural member 60 illustrated for example in FIG. 8, and a planar sheet or film of polymeric material 74, preferably including a plurality of apertures 88, as will be explained further below. The polymeric material can be attached to an existing stent structural member by tightly wrapping the polymer film at least once, and preferably multiple times, circumferentially around the stent structural member 72 in an unexpanded state to form a coil of layers of the polymeric material. The film of polymeric material in this embodiment has an interior end 76, multiple wrappings forming a plurality of layers 77 of the polymeric material, and an exterior end 78 overlapping the multiple layers. The coil of polymeric material preferably is secured snugly over the stent structure by at least one piece or strip of elastic material 80. One end 82 of at least one such piece or strip of elastic material is attached to the exterior end portion 78 of the coil of polymeric material, and an opposing end 83 of the piece of elastic material is attached to another portion 84 of the exterior of the wrapped coil of polymeric material, across the edge of the exterior end portion 78 of the coil of polymeric material, to secure the coil on the stent. In one currently preferred embodiment illustrated in FIGS. 9-11, the coil of polymeric material advantageously can be secured on the stent structural member by two strips of such elastic material. Additional strips of elastic material also can be used to secure the coil of polymeric material, as needed. The elastic material stretches to allow the coil of polymeric material to uncoil as the stent is expanded. In a currently preferred embodiment, the strips of elastic material are heat-bonded to the coil of polymeric material. Attachment of the elastic material also can be accomplished by adhesive bonding, solvent bonding, or by one or more mechanical fasteners, such as with a metal clip, for example. In this embodiment, the planar sheet of polymeric material preferably is wrapped circumferentially

and cinched tightly as a sleeve around the stent structural member, and thus is attached to the stent structural member by an interference fit.

[0025] In a currently preferred alternative embodiment shown in FIGS. 12 and 13, similar to that illustrated in FIGS. 9-11, the elastic strip of material 80 can extend and be bonded along the entire width of the exterior end 78 of the coil of polymeric material as is shown in FIG. 12, and can be bonded to the other portion 84 of the exterior of the wrapped coil of polymeric material, across the edge of the exterior end portion 78 of the coil of polymeric material, to secure the coil on the stent, as is illustrated in FIG. 13. The strip of elastic material also can be perforated, such as with apertures 86 formed in the strip of elastic material for example, to decrease the cross-sectional area of the elastic material and thus to permit the elastic material to stretch more easily. The polymeric film material also currently preferably includes a plurality of apertures 88 so that the polymeric material is porous, to allow blood to flow through the stent structural member 72 to the vessel wall, such as for oxygenation of and nutrient exchange with the vessel wall, and in order to present a decreased surface area for purposes of reducing thrombogenicity. The apertures also improve the flexibility of the polymeric material, allowing the stent segment to be more easily rolled and uncoiled during expansion of the stent structural member, and also facilitate the process of cell growth over the surface of the stent.

[0026] The primary function of the sheet of polymeric material 24,44,74 is to deliver therapeutic agents or drugs to help prevent thrombosis and/or restenosis. The planar sheet of polymeric material preferably is selected from the group of polymers consisting of thermoplastic and elastomeric polymers, that however can be substantially inelastic, so as not to lose a significant part of their thickness during expansion of the stent structural member, such as polycaprolactone, for example, allowing a high upper threshold for the amount of one or more drugs that can be loaded in the polymeric material and delivered. The inelastic polymeric material currently preferred is of a thickness that will guarantee drug delivery over at least approximately a seven-day period, which currently is not possible with radially-expanding elastic films. In the embodiment illustrated in FIGS. 9-13, an inelastic drug-loaded polymeric material is currently preferred which is no greater than about 0.0508 millimeter (0.002 inch) thick, and typically approximately is 0.0381 to 0.0508 millimeter (0.0015 inch to 0.002 inch) thick, to prevent the profile of the stent and wrap of polymeric material from becoming too large. The elastic portion of the sleeve of polymeric material keeps the coiled polymeric film secured snugly over the expandable stent structural member, so that the polymeric material can be applied over the stent structural member without the need for additional internal points of attachment to the stent structural member. The elastic portion of the sleeve of polymeric material also keeps tension on the

coiled, inelastic drug-containing material while the stent structural member is expanding, without providing so much resistance so as to impede expansion of the stent structural member, or the unrolling of the inelastic polymeric material.

[0027] The elastic strip of material can be joined on the interior or exterior of the end portion of the coiled polymeric material. The elastic material attached over the coil of polymeric material helps keep the coil of drug-loaded material snug on the stent structural member before it is expanded, and guides its linear expansion during inflation of a balloon dilatation catheter used for deployment of the stent and polymeric drug-loaded material in the vasculature or other body lumen of a patient.

[0028] The elastic material currently typically is formed of ethylene vinyl acetate, but also can also be formed of silicone polymers. The drug-loaded layer of polymeric material and the stent structural member can be formed of the materials as described above in the previous embodiments.

[0029] In another alternative embodiment illustrated in FIGS. 14-16, another preferred type of stent 90 that can be drug-loaded comprises a stent metal structural member 92, that, for example, can be a slotted tube type of stent having a plurality of slotted openings 91 and structural ribs 93 as is illustrated in FIG. 16, such as is available from Advanced Cardiovascular Systems, in combination with a planar sheet or film of polymeric material 94. The stent structural member also can be other types of stents that preferably have a relatively significant proportion of space provided by openings, slots, or the like in the otherwise solid material of the stent structure. The polymeric material can be attached to such a stent structural member by tightly wrapping the polymer film at least once, and preferably multiple times, circumferentially around the stent structural member 92 in an unexpanded state to form a coil of layers of the polymeric material. The film of polymeric material in this embodiment has an interior end 96 with at least one attachment member or tab 100 adapted to be received in openings 91 of the stent structural member and thereby attached to the stent structural member, and provides multiple wrappings forming a plurality of layers 97 of the polymeric material, with an exterior end 98 overlapping the interior multiple layers. As is shown in FIG. 14, the polymeric film of material currently preferred has a plurality of attachment tabs 100, and typically has two of such attachment tabs. Each attachment tab currently preferably includes an aperture 101 therethrough, which is adapted to receive and to hook onto a structural rib portion 93 of the stent structural member. The attachment tab also includes a slit 102 extending from the aperture 101 to the outer edge 103 of the attachment tab, to allow the attachment tab to be hooked onto the stent structural member. After the attachment tab is hooked onto a portion of the stent structural member, the slit 102 preferably is sealed closed, such as by application of an adhesive material, typically a copolymer of poly-L-lactic acid

(L-PLA) and polycaprolactone (PCL), other suitable adhesives, or by heat bonding. The coil of polymeric material preferably is formed of a thermoplastic material such as polycaprolactone that can be drug-loaded, and can be wrapped and secured snugly over the stent structure by heat bonding the exterior end 98 to another portion of the exterior of the wrapped coil of polymeric material as described above. The polymeric film of material tensions the attachment tabs as the stent structural member is expanded and as the wrapping of polymeric material uncoils, to bias the attachment tab extending into the lumen of the stent structural member against the inner surface of the lumen of the stent structural member to insure that the attachment tabs do not obstruct the lumen within the stent structural member. Attachment of the exterior edge of the polymeric material to the wrapping of polymeric material currently preferably is accomplished by adhesive bonding, typically by an adhesive such as a copolymer of poly-L-lactic acid (L-PLA) and polycaprolactone (PCL), although other adhesives, heat bonding, solvent bonding, or one or more mechanical fasteners, such as with a metal clip, for example, may also be suitable.

[0030] In a currently preferred embodiment, the polymeric film material typically is about 0.0508 millimeter (about 0.002 inch) thick, and also currently preferably includes a plurality of apertures 108 so that the polymeric material is porous, to allow blood to flow through the stent structural member to the vessel wall, such as for oxygenation and nutrient exchange to the vessel wall, and in order to present a decreased surface area for purposes of reducing thrombogenicity. The apertures also improve the flexibility of the polymeric material, allowing the stent segment to be more easily rolled and uncoiled during expansion of the stent structural member, and also to facilitate the process of cell growth over the surface of the stent.

[0031] The primary function of the sheet of polymeric material is to deliver therapeutic agents or drugs to help prevent thrombosis and/or restenosis. The planar sheet of polymeric material preferably is selected from the group of polymers consisting of thermoplastic and elastomeric polymers that may be inelastic, and that do not lose a significant part of their thickness during expansion of the stent structural member, allowing a high upper threshold for the amount of one or more drugs that can be loaded in the polymeric material and delivered. As is illustrated in FIGS. 15 and 16, the drug-loaded stent can be mounted on an expandable balloon member 110 of a dilatation catheter 112, near radiopaque markers 114 of the catheter, for delivery of the stent in an artery, other blood vessel, or other body lumen, such as through a protective sheath 116, shown cutaway for convenience of illustration.

[0032] In another currently preferred embodiment illustrated in FIGS. 17-18, a combination of a stent structural member and a polymeric film wrapping can be provided with a coating of lubricious material 120. The lu-

bricous material currently preferred is a mixture of polyethylene oxide and polyethylene glycol, providing both high and low molecular weight components in the lubricious material, although other types of hydrophilic polymeric materials such as polyethylene acetate, polyvinyl pyrrolidone (PVP), polyvinyl alcohol, polyacrylamide, hydrophilic soft segment urethanes, some natural gums such as gum arabic or gum tragacanth and the like, polyanhydrides or other similar hydrophilic polymers, and combinations thereof, also can be used. The lubricious material also can carry an anti-thrombogenic drug that can be the same as, or complementary to, the anti-thrombogenic or anti-proliferative drug or drugs carried in the polymeric material of the stent.

[0033] The lubricious coating currently preferably is applied over a stent-and-polymer-film-wrap combination by dipping the wrapped stent in the hydrated, liquid lubricious material. The lubricious material typically is prepared to be sufficiently viscous to allow the stent to be coated sufficiently by a single dipping. The lubricious coating initially is quite sticky when applied, but it is dried to provide a non-sticky tight cocoon around the wrapped stent, and helps to keep the polymer wrapping tight. While the lubricious coating is shown applied to a wrapped stent such as that of FIGS. 14-16, the lubricious coating advantageously can be applied to any of the foregoing wrapped stent combinations, and other suitable stents as well. The lubricious coating becomes hydrated again upon exposure to the blood during delivery of the stent. When a sheath is used in the delivery system to protect the stent during delivery, the lubricious coating initially can be hydrated before contacting the blood by flushing the sheath with saline solution. Due to the gel-like nature of the lubricious coating, the lubricious coating eventually dissolves in a short period of time, and typically will be completely degraded and dissolved by the time the stent is deployed and expanded.

[0034] The layer of lubricious material protects the stent from the guide catheter or the anatomy by providing a low friction surface over the stent. If a sheath or sleeve is used for delivering the stent, the lubricious coating aids in retraction of the sheath by decreasing friction between internal and external layers of the delivery system. The deployment of the stent also can be improved by decreasing friction between the stent and the balloon used to deliver the stent, decreasing friction between the layers of the stent itself, or decreasing friction between the vessel or lumen wall and the stent. The need for a sheath for protecting the stent during delivery also can be mitigated if the coating is of a thickness suited to providing a smooth transition through the delivery system, and still provides a low profile of the uninflated, undeployed stent. Alternatively, the lubricious coating also can be formed as a dried sheet of lubricious material, cut into a strip, wrapped in spiral fashion over the length of the polymeric drug carrying wrapping, and bonded in place by an adhesive such as a copolymer of poly-L-lactic acid (L-PLA) and polycaprolactone (PCL),

although other adhesives, or heat bonding may also be suitable.

[0035] It thus has been demonstrated that the described embodiments provide a stent — combining polymeric materials with stent structures with the capability of absorbing therapeutic drugs or other agents, for placement and release of the therapeutic agents at a specific intravascular site. A complex locking design is not needed, and the stent can be re-dilated if necessary. The polymeric, drug-containing section can be bioabsorbable, and can be specially formulated for its specific function of delivering drugs locally, since it is not necessary for the polymeric component to provide assistance in keeping the blood vessel open. The polymeric material can be extruded as a film, using simple technology, and can be processed while the material is a flat sheet. The stent can be used in coronary arteries or any other part of the vasculature where mechanical opening force is necessary or desirable to keep the vessel open, and where anti-restenosis, anti-proliferative or other types of therapeutic drugs or agents can be useful in combating thrombosis and restenosis.

[0036] It therefore will be apparent from the foregoing that while particular forms of the invention have been illustrated and described, various modifications can be made without departing from the scope of the invention.

Claims

1. A drug-loaded stent (20), comprising: an expandable stent structural member (22); and a polymeric material disposed on the stent structural member (22), the polymeric material being loaded with a therapeutic agent, characterised in that the polymeric material is a planar sheet (24) wrapped in a coil around the stent structural member (22).
2. The drug-loaded stent (20) of claim 1, wherein said planar sheet (24) of polymeric material is wrapped circumferentially around the stent structural member (22) at least one time, and said planar sheet (24) of polymeric material is attached to itself.
3. The drug-loaded stent (20) of claim 1, wherein said planar sheet (24) of polymeric material is wrapped circumferentially around the stent structural member (22) at least one time, and said planar sheet (24) of polymeric material is attached to the stent structural member (22) by interference fit.
4. The drug-loaded stent (20) of claim 1, wherein said planar sheet (24) of polymeric material is wrapped circumferentially around the stent structural member (22) at least one time, and said planar sheet (24) of polymeric material is attached to the stent structural member (22) by adhesive.
5. The drug-loaded stent (20) of claim 1, wherein said stent structural member (22) has a surface defining a plurality of slotted openings (91) therethrough and a plurality of structural ribs (93), said planar sheet (24) of polymeric material has at least one attachment tab (100) having an aperture (101) therethrough and a slit (102) extending from said aperture (101) to an outside edge (103) of said attachment tab (100), said planar sheet (24) of polymeric material being attached to the stent structural member (22) by inserting said attachment tab (100) into one said slotted opening (91) and hooking said slit (102) and said aperture (101) of said attachment tab (100) to a structural rib (93) of said stent structural member (22), and said sheet (24) of polymeric material is wrapped circumferentially around the stent structural member (22) at least one time.
6. The drug-loaded stent (20) of any preceding claim, wherein said planar sheet (24) of polymeric material is selected from the group of polymers consisting of thermoplastic and elastomeric polymers, whereby said sheet (24) stretches radially when said stent structural member (22) is expanded.
7. The drug-loaded stent (20) of any of claims 1, 4 or 5, wherein said planar sheet (24) of polymeric material is adapted to uncoil and expand to substantially match the expansion of said stent structural member (22).
8. The drug-loaded stent (20) of any of claims 1, 4, 5 or 7, wherein said stent structural member (22) has a longitudinal axis (32), and said planar sheet (24) of polymeric material has at least one slit (30) transverse to the axis (32) of said stent structural member (22) to accommodate uneven expansion of the stent structural member (22).
9. The drug-loaded stent (20) of any preceding claim wherein said therapeutic agent is selected from the group consisting of therapeutic agents consisting of antiplatelets, antithrombins, cytostatic and antiproliferative agents.
10. The drug-loaded stent (20) of any preceding claim, wherein said therapeutic agent is selected from the group of therapeutic agents consisting of sodium heparin, low molecular weight heparin, hirudin, argatroban, forskolin, vapiprost, prostacyclin and prostacyclin analogues, dextran, D-phe-pro-arg-chloromethylketone, dipyridamole, glycoprotein IIb/IIIa platelet membrane receptor antibody, recombinant hirudin, thrombin inhibitor, angiopeptin, angiotensin converting enzyme inhibitors, calcium channel blockers, colchicine, fibroblast growth factor antagonists, fish oil, omega 3-fatty acid, histamine antagonists, HMG-CoA reductase inhibitor,

methotrexate, monoclonal antibodies, nitroprusside, phosphodiesterase inhibitors, prostaglandin inhibitor, serotonin blockers, steroids, thioprotease inhibitors, triazolopyrimidine, PDGF antagonists, alpha-interferon, genetically engineered epithelial cells, and combinations thereof.

11. The drug-loaded stent (20) of any preceding claim, wherein said stent structural member (22) is formed from a metal selected from the group of metals consisting of stainless steel, tantalum, nickel-titanium alloy, platinum-iridium alloy, gold, magnesium, MP35N, and MP20N.

12. The drug-loaded stent (20) of any preceding claim, wherein said planar sheet (24) of polymeric material has a surface defining a plurality of openings (34) to promote rapid endothelialization.

13. The drug-loaded stent (20) of any preceding claim, wherein said planar sheet (24) of polymeric material is coated with a layer of hydrophilic lubricious polymeric material (120).

14. The drug-loaded stent (20) of claim 13, wherein said lubricious material (120) is selected from the group consisting of polyethylene oxide, polyethylene glycol, polyethylene acetate, polyvinyl pyrrolidone, polyvinyl alcohol, polyacrylamide, hydrophilic soft segment urethane, gum arabic, gum tragacanth and combinations thereof.

Patentansprüche

1. Medikamentenhaltiger Stent (20), umfassend ein expandierbares Stentstrukturelement (22) sowie ein auf dem Stentstrukturelement (22) angeordnetes Polymermaterial, wobei das Polymermaterial mit einem therapeutischen Mittel beladen ist, **dadurch gekennzeichnet**, dass das Polymermaterial eine flache Schicht (24) ist, die in einem Wickel um das Stentstrukturelement (22) herumgewickelt ist.

2. Medikamentenhaltiger Stent (20) nach Anspruch 1, wobei die flache Schicht (24) aus Polymermaterial zumindest einmal über den Umfang des Stentstrukturelements (22) herumgewickelt ist und wobei die flache Schicht (24) aus Polymermaterial an sich selbst befestigt ist.

3. Medikamentenhaltiger Stent (20) nach Anspruch 1, wobei die flache Schicht (24) aus Polymermaterial zumindest einmal über den Umfang um das Stentstrukturelement (22) herumgewickelt ist und wobei die flache Schicht (24) aus Polymermaterial durch Presssitz an dem Stentstrukturelement (22) befestigt ist.

4. Medikamentenhaltiger Stent (20) nach Anspruch 1, wobei die flache Schicht (24) zumindest einmal über den Umfang des Stentstrukturelements (22) herumgewickelt ist, wobei die flache Schicht (24) aus Polymermaterial durch Klebstoff an dem Stentstrukturelement (22) angebracht ist.

5. Medikamentenhaltiger Stent (20) nach Anspruch 1, wobei das Stentstrukturelement (22) eine Oberfläche aufweist, die eine Mehrzahl geschlitzter Durchgangsöffnungen (91) sowie eine Mehrzahl von Strukturrippen (93) definiert, wobei die flache Schicht (24) aus Polymermaterial zumindest eine Halterungslasche (100) aufweist, die eine Durchgangsöffnung (101) und einen Schlitz (102) aufweist, der sich von der Öffnung (101) zu einem Außenrand (103) der Halterungslasche (100) erstreckt, wobei die flache Schicht (24) aus Polymermaterial an dem Stentstrukturelement (22) angebracht ist, indem die Halterungslasche (100) in eine der geschlitzten Öffnungen (91) eingesetzt wird und der Schlitz (102) und die Öffnung (101) der Halterungslasche (100) an eine Strukturrippe (93) des Stentstrukturelements (22) verhakt werden, und wobei die Schicht (24) aus Polymermaterial zumindest einmal über den Umfang des Stentstrukturelements (22) herumgewickelt ist.

6. Medikamentenhaltiger Stent (20) nach einem der vorhergehenden Ansprüche, wobei die flache Schicht (24) aus Polymermaterial aus der Gruppe von Polymeren gewählt ist, die aus thermoplastischen und elastomeren Polymeren besteht, wodurch sich die Schicht (24) radial streckt, wenn das Stentstrukturelement (22) expandiert wird.

7. Medikamentenhaltiger Stent (20) nach einem der Ansprüche 1, 4 oder 5, wobei die flache Schicht (24) aus Polymermaterial dazu ausgelegt ist, sich abzuwickeln und zu expandieren, um sich der Expansion des Stentstrukturelements (22) im Wesentlichen anzupassen.

8. Medikamentenhaltiger Stent (20) nach einem der Ansprüche 1, 4, 5 oder 7, wobei das Stentstrukturelement (22) eine Längsachse (32) aufweist, und wobei die flache Schicht (24) aus Polymermaterial zumindest einen Schlitz (30) quer zur Achse (32) des Stentstrukturelements (22) aufweist, um eine ungleichmäßige Expansion des Stentstrukturelements (22) aufzunehmen.

9. Medikamentenhaltiger Stent (20) nach einem der vorhergehenden Ansprüche, wobei das therapeutische Mittel aus der Gruppe ausgewählt ist, die aus therapeutischen Mitteln besteht, die aus Antiplatelets, Antithrombinen, cytostatischen und antiproliferativen Mitteln besteht,

10. Medikamentenhaltiger Stent (20) nach einem der vorhergehenden Ansprüche, wobei das therapeutische Mittel aus der Gruppe therapeutischer Mittel ausgewählt ist, bestehend aus Natriumheparin, Heparin mit niedrigem Molekulargewicht, Hirudin, Argatroban, Forskolin, Vapiprost, Prostacyclin und Prostacyclinanaloge, Dextran, D-phe-pro-arg-Chlormethylketon, Dipyridamol, Glykoprotein IIb/IIIa Plateletmembran-Rezeptorantikörper, rekombinantes Hirudin, Thrombininhibitor, Angiopeptin, Angiotensin-wandelnde Enzyminhibitoren, Calciumkanalblocker, Colchicin, Fibroblastenwachstumsfaktor-Antagonisten, Fischöl, omega 3-Fettsäure, Histaminantagonisten, HMG-CoA Reduktaseinhibitor, Methotrexat, monoklonale Antikörper, Nitroprussid, Phosphodiesteraseinhibitoren, Prostaglandininhibitor, Serotoninblocker, Steroide, Thioproteaseinhibitoren, Triazolpyrimidin, PDGF-Antagonisten, alpha-Interferon, gentechnisch behandelte Epithelzellen und Kombinationen davon.

11. Medikamentenhaltiger Stent (20) nach einem der vorhergehenden Ansprüche, wobei das Stentstrukturelement (22) aus einem Material gebildet ist, das aus der Gruppe von Metallen gewählt ist, die aus rostfreiem Stahl, Tantal, Nickeltitanlegierung, Platiniridiumlegierung, Gold, Magnesium, MP35N und MP20N besteht.

12. Medikamentenhaltiger Stent (20) nach einem der vorhergehenden Ansprüche, wobei die flache Schicht (24) aus Polymermaterial eine Oberfläche aufweist, die eine Mehrzahl von Öffnungen (34) definiert, um eine schnelle Endothelisierung zu fördern.

13. Medikamentenhaltiger Stent (20) nach einem der vorhergehenden Ansprüche, wobei die flache Schicht (24) aus Polymermaterial mit einer Schicht aus hydrophilem schmierfähigem Polymermaterial (120) beschichtet ist.

14. Medikamentenhaltiger Stent (20) nach Anspruch 13, wobei das Schmiermaterial (120) aus der Gruppe gewählt ist, die aus Polyethylenoxid, Polyethylenglykol, Polyethylenacetat, Polyvinylpyrrolidon, Polyvinylalkohol, Polyacrylamid, hydrophiles Weichsegmenturethan, Gummi arabicum, Tragantgummi und Kombinationen davon besteht.

Revendications

1. Stent garni de médicament (20), comprenant un élément structural de stent expansible (22) et un matériau polymère placé sur l'élément structural de stent (22), le matériau polymère étant chargé d'un agent thérapeutique, caractérisé en ce que le ma-

tériau polymère est une feuille plane (24) enroulée en spirale autour de l'élément structural de stent (22).

2. Stent garni de médicament (20) selon la revendication 1, dans lequel ladite feuille plane (24) de matériau polymère est enroulée au moins une fois autour de la circonférence de l'élément structural de stent (22), et ladite feuille plane (24) de matériau polymère est attachée à elle-même.

3. Stent garni de médicament (20) selon la revendication 1, dans lequel ladite feuille plane (24) de matériau polymère est enroulée au moins une fois autour de la circonférence de l'élément structural de stent (22), et ladite feuille plane (24) de matériau polymère est attachée à l'élément structural de stent (22) par ajustement serré.

4. Stent garni de médicament (20) selon la revendication 1, dans lequel ladite feuille plane (24) de matériau polymère est enroulée au moins une fois autour de la circonférence de l'élément structural de stent (22), et ladite feuille plane (24) de matériau polymère est attachée à l'élément structural de stent (22) par adhésif.

5. Stent garni de médicament (20) selon la revendication 1, dans lequel ledit élément structural de stent (22) a une surface présentant une pluralité d'ouvertures entaillées (91) à travers elle et une pluralité de nervures structurales (93), ladite feuille plane (24) de matériau polymère a au moins une patte de fixation (100) ayant un orifice (101) à travers elle et une fente (102) s'étendant depuis ledit orifice (101) jusqu'à un bord extérieur (103) de ladite patte de fixation (100), ladite feuille plane (24) du matériau polymère étant attachée à l'élément structural de stent (22) par insertion de ladite patte de fixation (100) dans l'une desdites ouvertures entaillées (91) et accrochage de ladite fente (102) et dudit orifice (101) de ladite patte de fixation (100) à une nervure structurale (93) dudit élément structural de stent (22), et ladite feuille (24) de matériau polymère est enroulée au moins une fois autour de la circonférence de l'élément structural de stent (22).

6. Stent garni de médicament (20) selon l'une quelconque des revendications précédentes, dans lequel ladite feuille plane (24) de matériau polymère est choisie dans le groupe de polymères comprenant des polymères thermoplastiques et élastomères, moyennant quoi ladite feuille (24) s'étire dans la direction radiale lorsque ledit élément structural de stent (22) est déployé.

7. Stent garni de médicament (20) selon l'une quelconque des revendications 1, 4 ou 5, dans lequel

ladite feuille plane (24) de matériau polymère est conçue pour se dérouler et s'élargir de façon à suivre essentiellement le déploiement dudit élément structural de stent (22).

8. Stent garni de médicament (20) selon l'une quelconque des revendications 1, 4, 5 ou 7, dans lequel ledit élément structural de stent (22) a un axe longitudinal (32), et ladite feuille plane (24) de matériau polymère a au moins une fente (30) transversale à l'axe (32) dudit élément structural de stent (22), pour contenir un déploiement inégal de l'élément structural de stent (22). 5
9. Stent garni de médicament (20) selon l'une quelconque des revendications précédentes, dans lequel ledit agent thérapeutique est choisi dans le groupe comprenant des agents thérapeutiques tels que des agents antiplaquettaires, antithrombotiques, cytostatiques et antiprolifératifs. 10
10. Stent garni de médicament (20) selon l'une quelconque des revendications précédentes, dans lequel ledit agent thérapeutique est choisi dans le groupe d'agents thérapeutiques suivants : héparine sodique, héparine à faible poids moléculaire, hirudine, argatroban, forskolin, vaspiprostan, prostacycline et analogues des prostacyclines, dextran, D-phosphoryl-arginine, chlorométhylcétone, dipyridamole, anticorps contre les récepteurs des membranes plaquettaires des glycoprotéines IIb/IIIa, hirudine recombinante, inhibiteur de la thrombine, angiotensine, inhibiteurs de l'enzyme de conversion de l'angiotensine, agents bloquants des canaux à calcium, colchicine, antagonistes du facteur de croissance des fibroblastes, huile de poisson, acide gras oméga 3, antagonistes de l'histamine, inhibiteurs de la HMG-CoA réductase, méthotrexate, anticorps monoclonaux, nitroprusside, inhibiteurs de la phosphodiesterase, inhibiteur de la prostaglandine, agents bloquants de la sérotonine, stéroïdes, inhibiteurs des thypotéases, triazolopyrimidine, antagonistes du PDGF, interféron alpha, cellules épithéliales traitées par génie génétique, et des combinaisons de ces agents. 15
11. Stent garni de médicament (20) selon l'une quelconque des revendications précédentes, dans lequel ledit élément structural de stent (22) est formé d'un métal choisi dans le groupe de métaux comprenant l'acier inoxydable, le tantale, un alliage nickel-titane, un alliage platine-iridium, l'or, le magnésium, le MP35N, et le MP20N. 20
12. Stent garni de médicament (20) selon l'une quelconque des revendications précédentes, dans lequel ladite feuille plane (24) de matériau polymère a une surface définissant une pluralité d'ouvertures 25

(34) pour favoriser une endothélialisation rapide.

13. Stent garni de médicament (20) selon l'une quelconque des revendications précédentes, dans lequel ladite feuille plane (24) du matériau polymère est revêtue d'une couche de matériau polymère onctueux hydrophile (120). 30
14. Stent garni de médicament (20) selon la revendication 13, dans lequel ledit matériau onctueux (120) est choisi dans le groupe comprenant l'oxyde de polyéthylène, le polyéthylène glycol, l'acétate de polyéthylène, la polyvinylpyrrolidone, l'alcool polyvinylique, le polyacrylamide, l'uréthane à segments mous hydrophiles, la gomme arabique, la gomme adragante, et des combinaisons de ceux-ci. 35

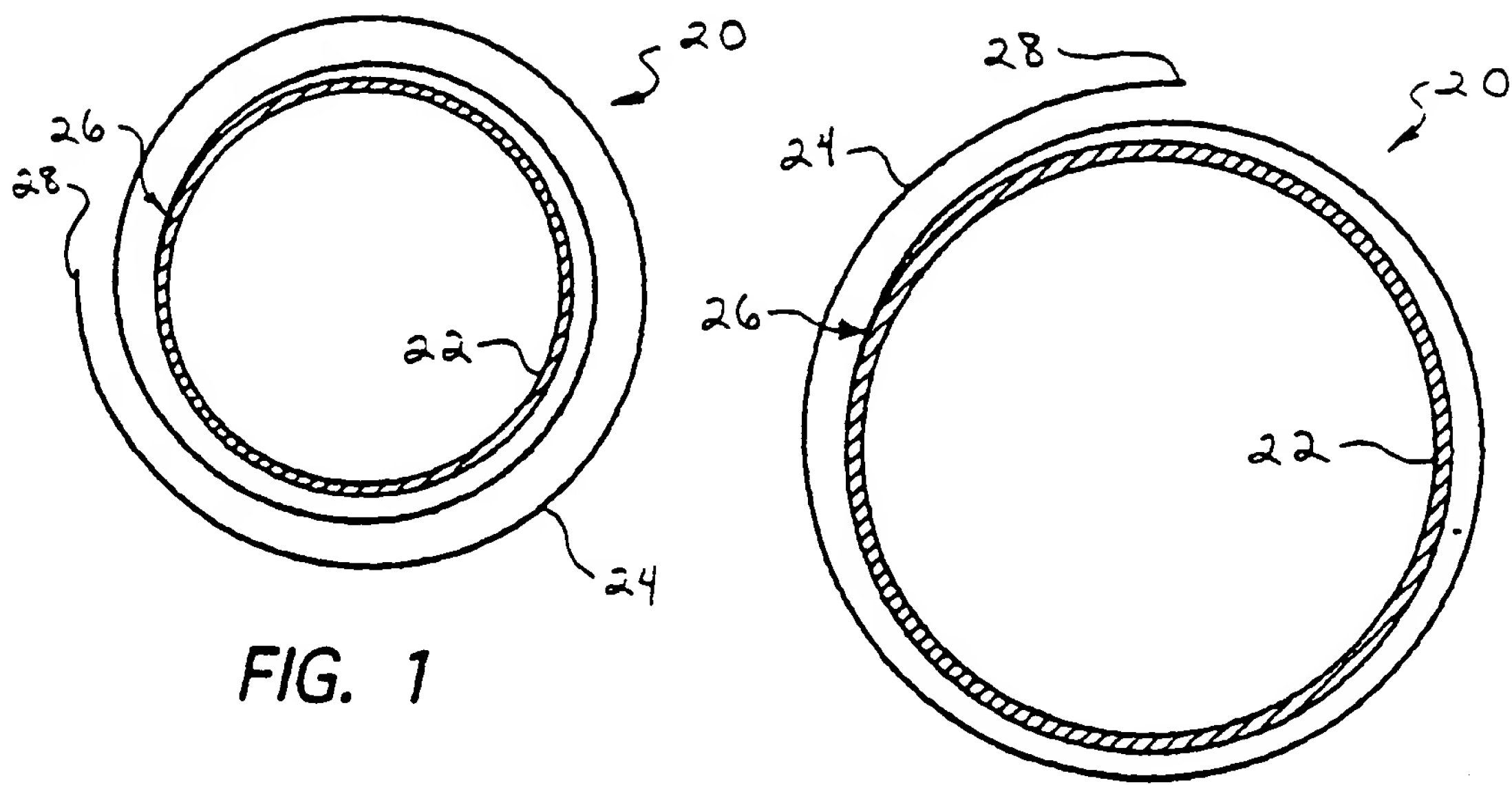


FIG. 1

FIG. 2

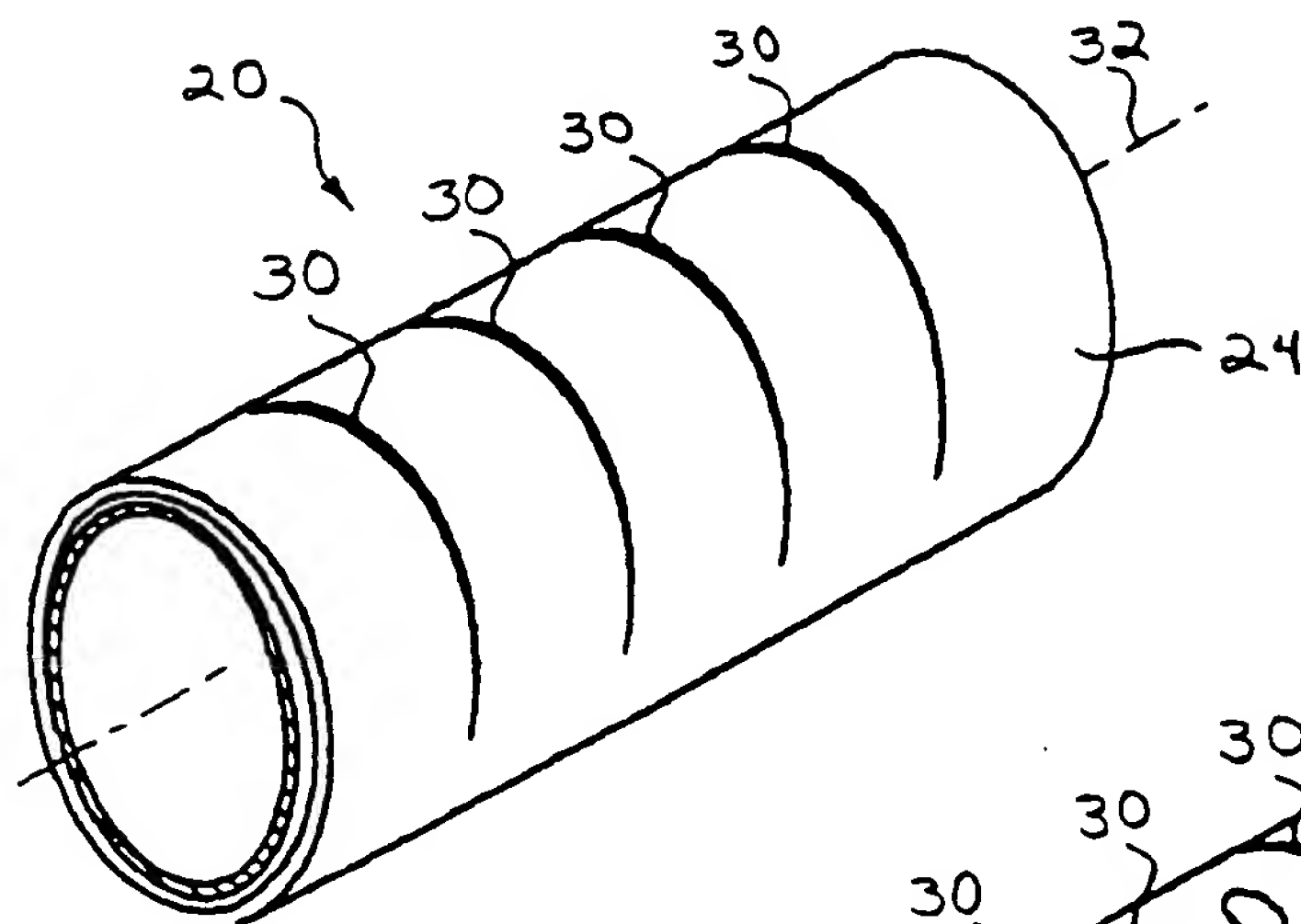


FIG. 3

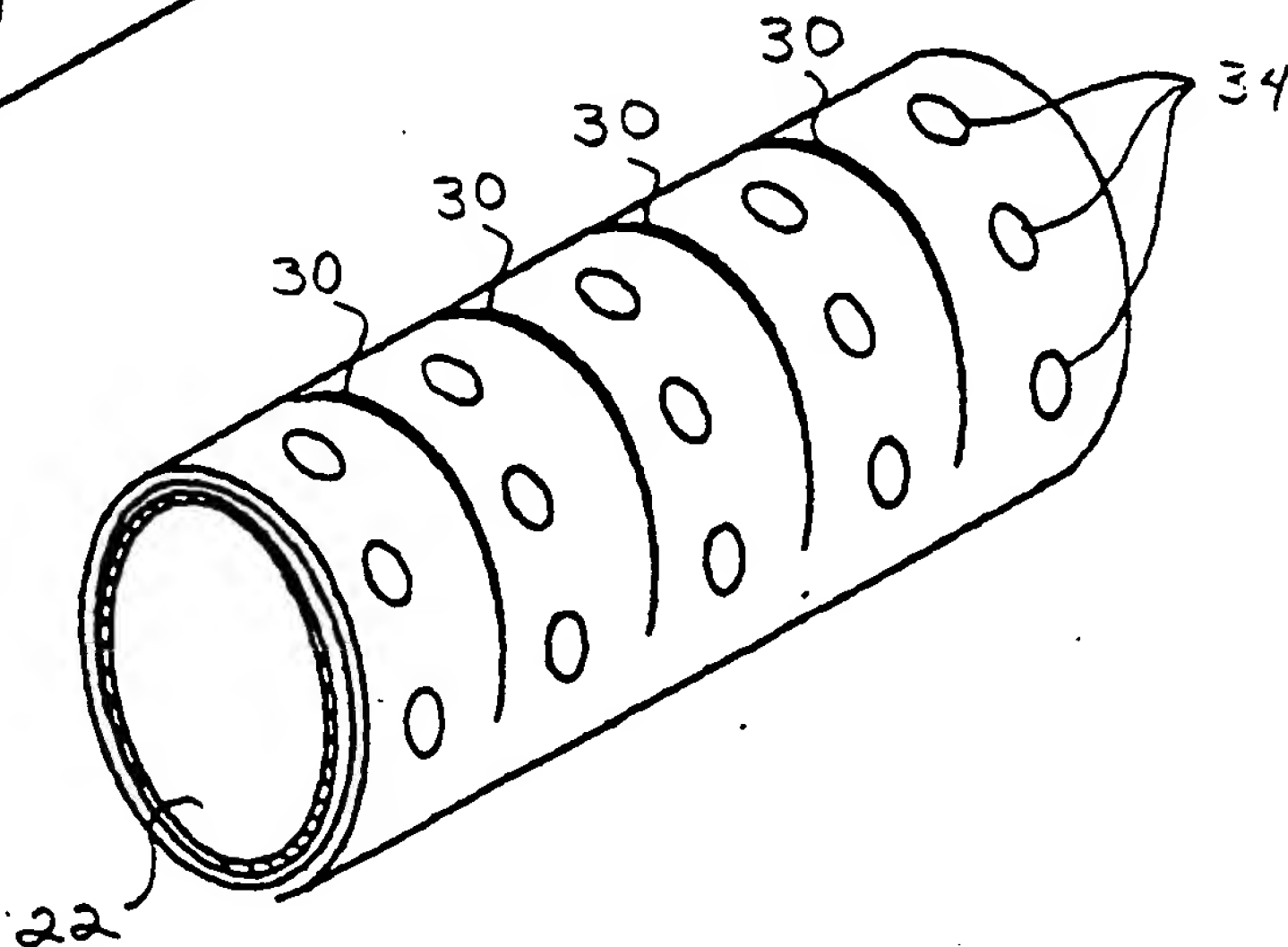


FIG. 4

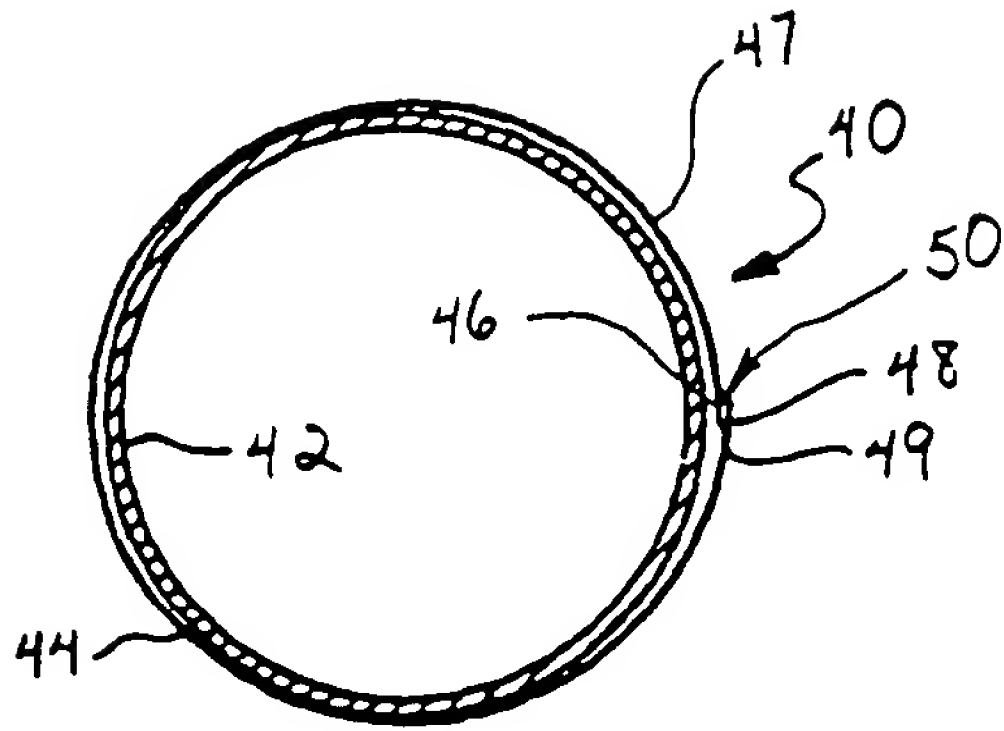


FIG. 5

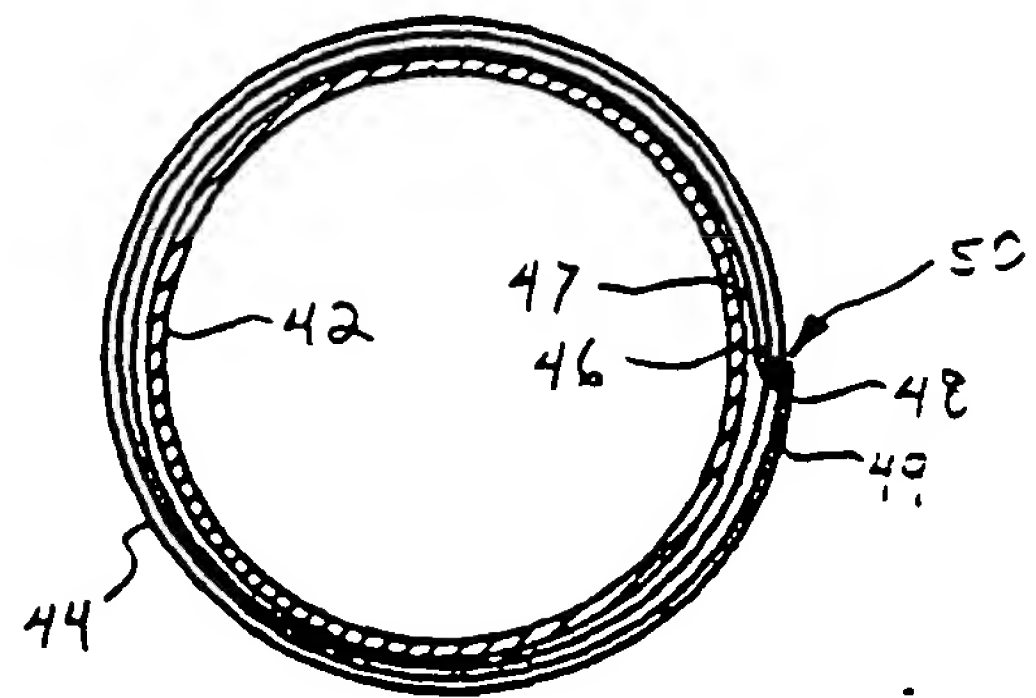


FIG. 7

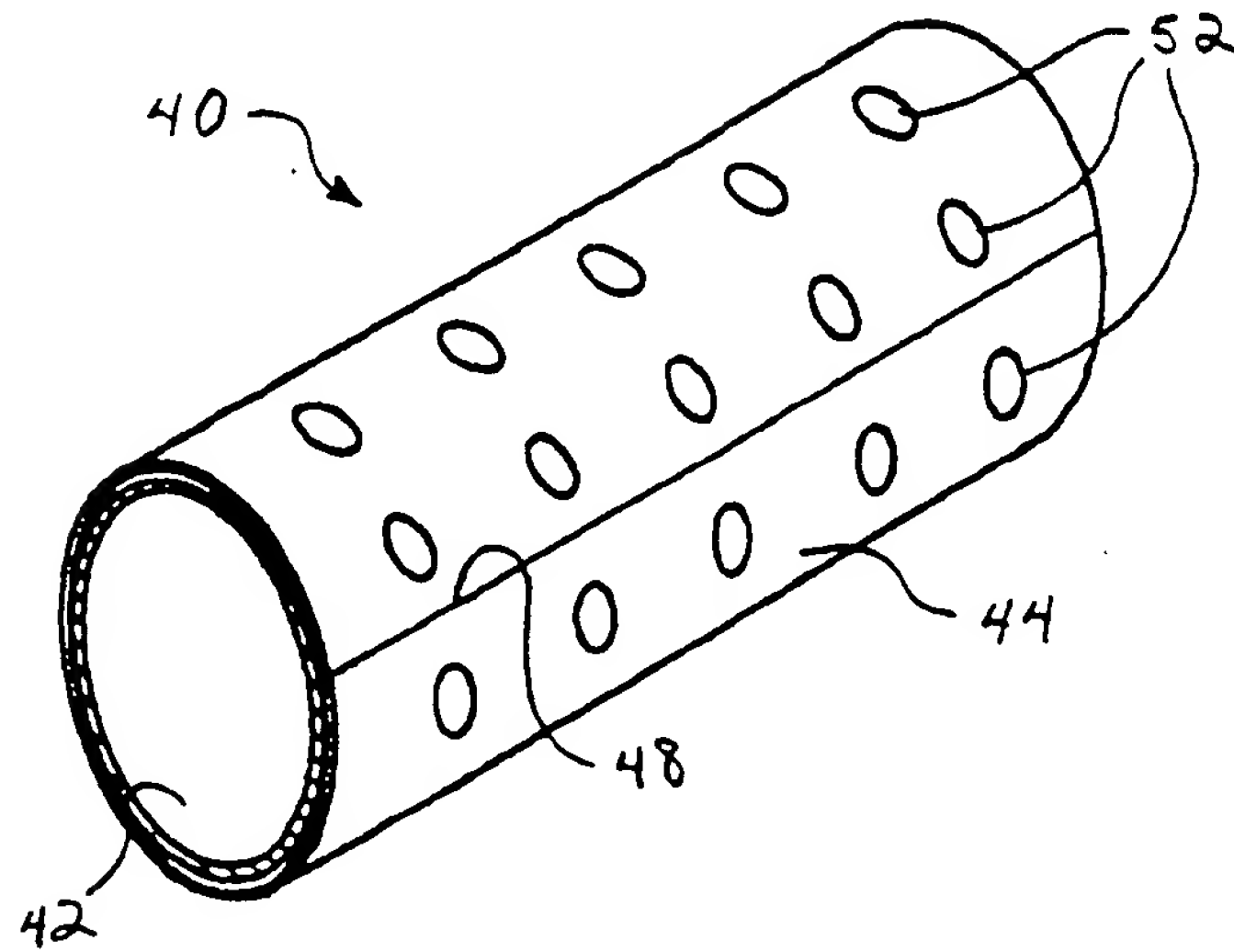


FIG. 6

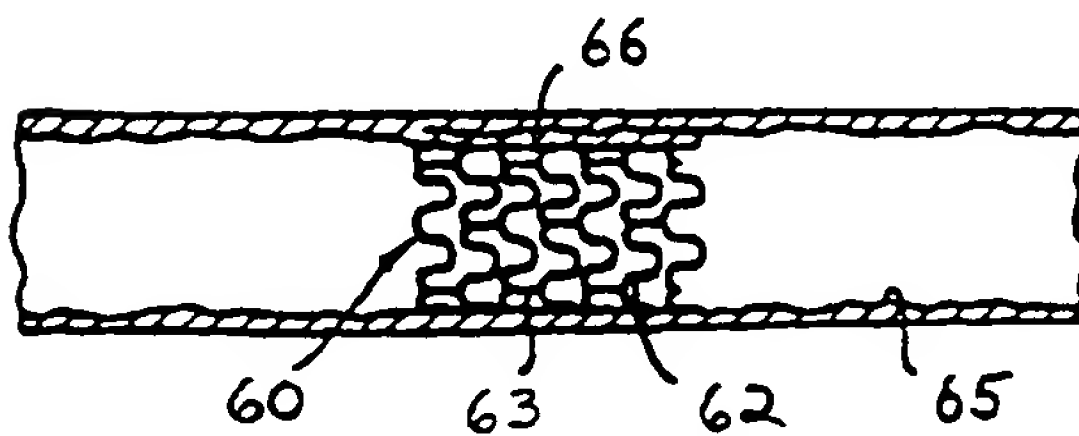


FIG. 8

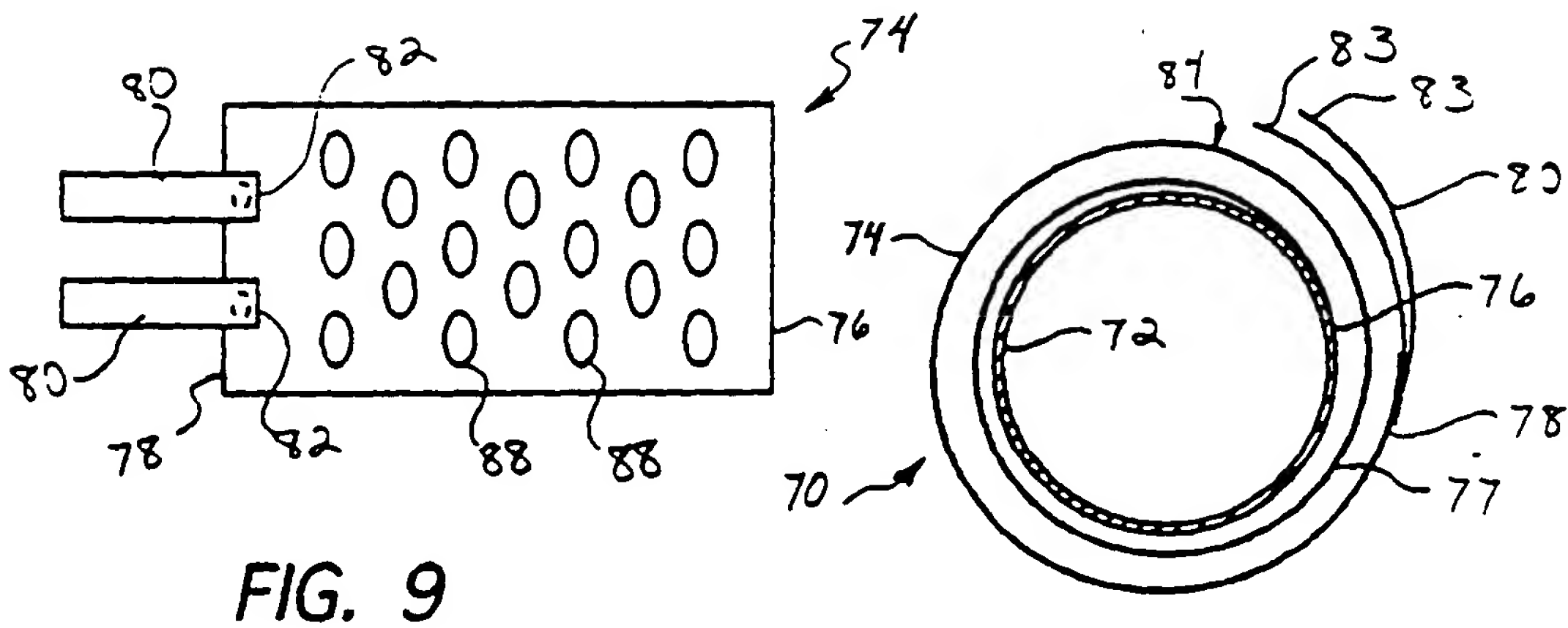


FIG. 10

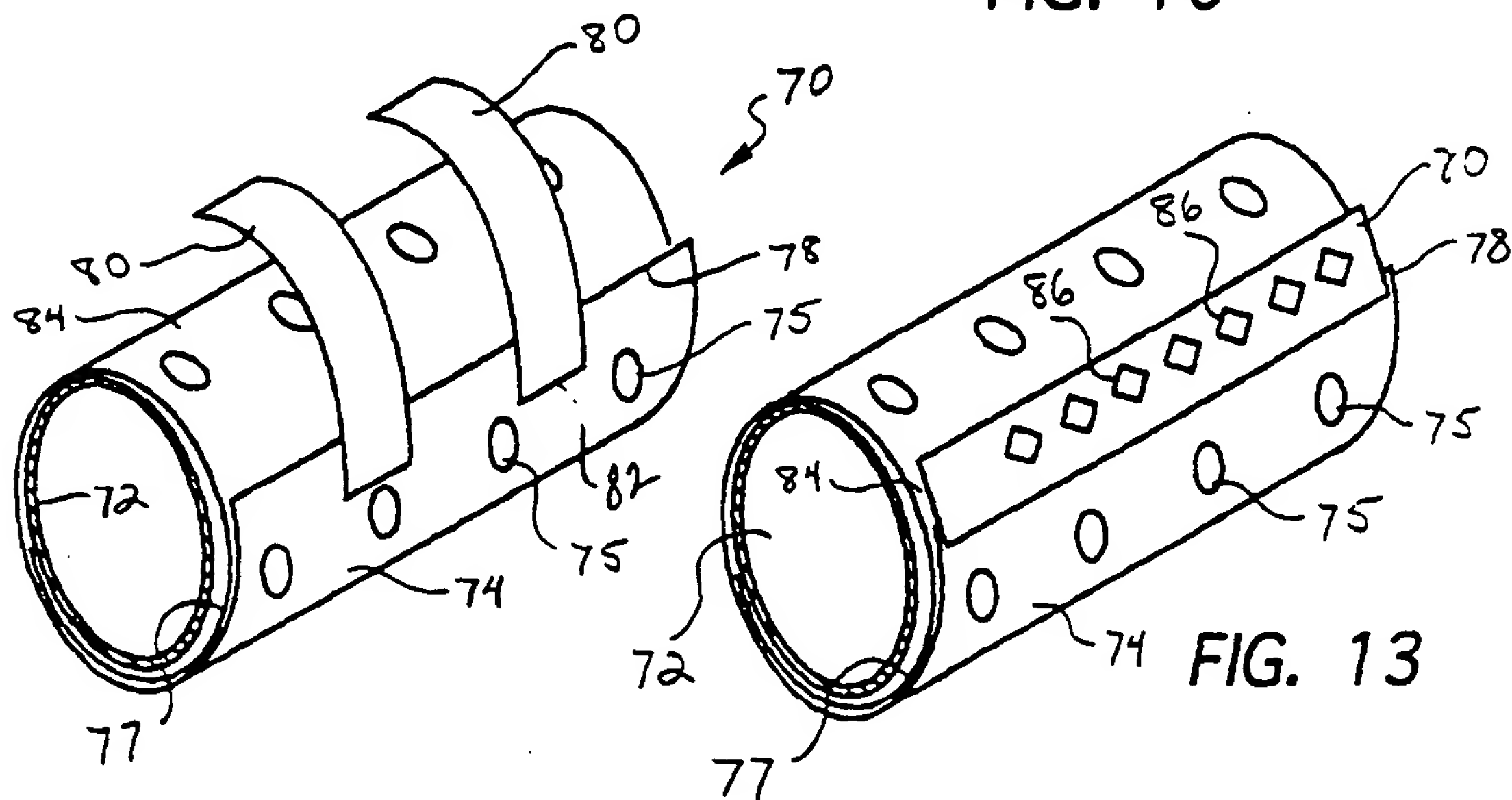
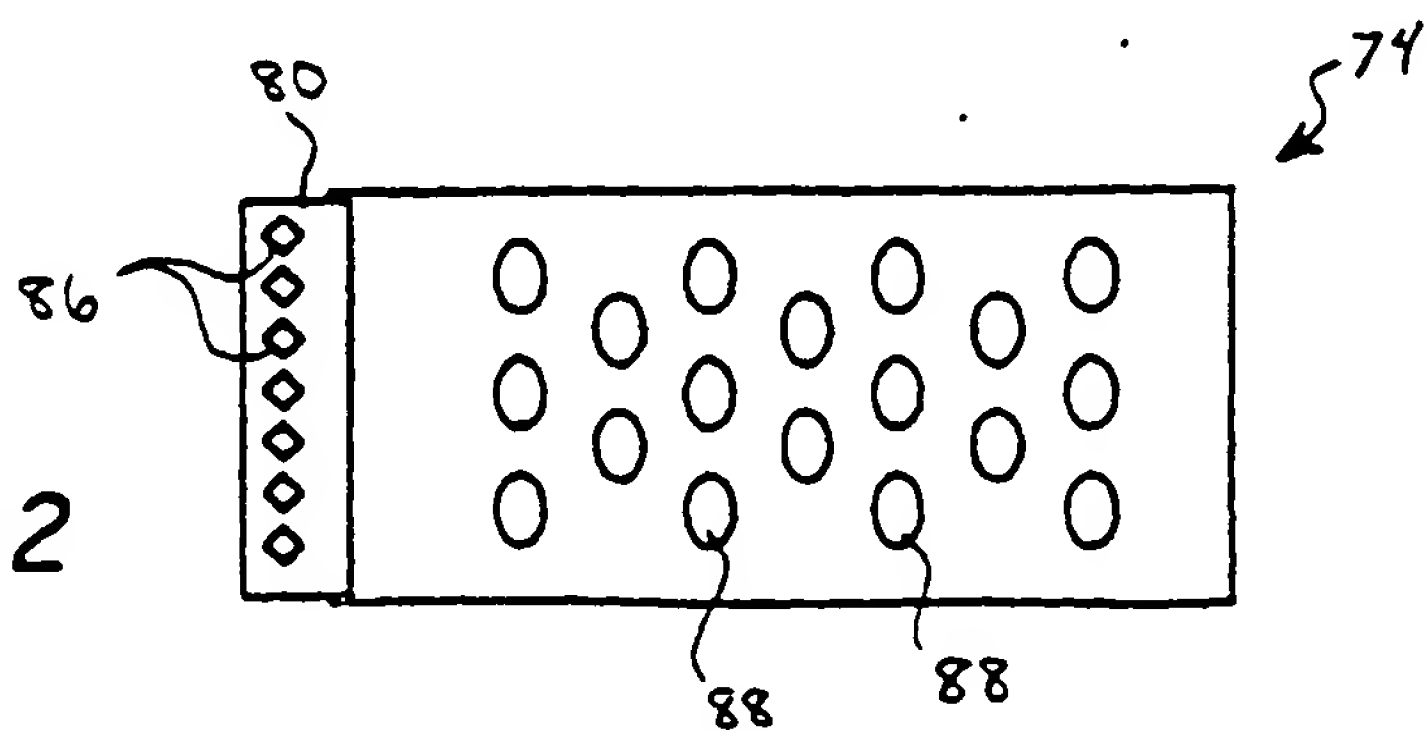


FIG. 12



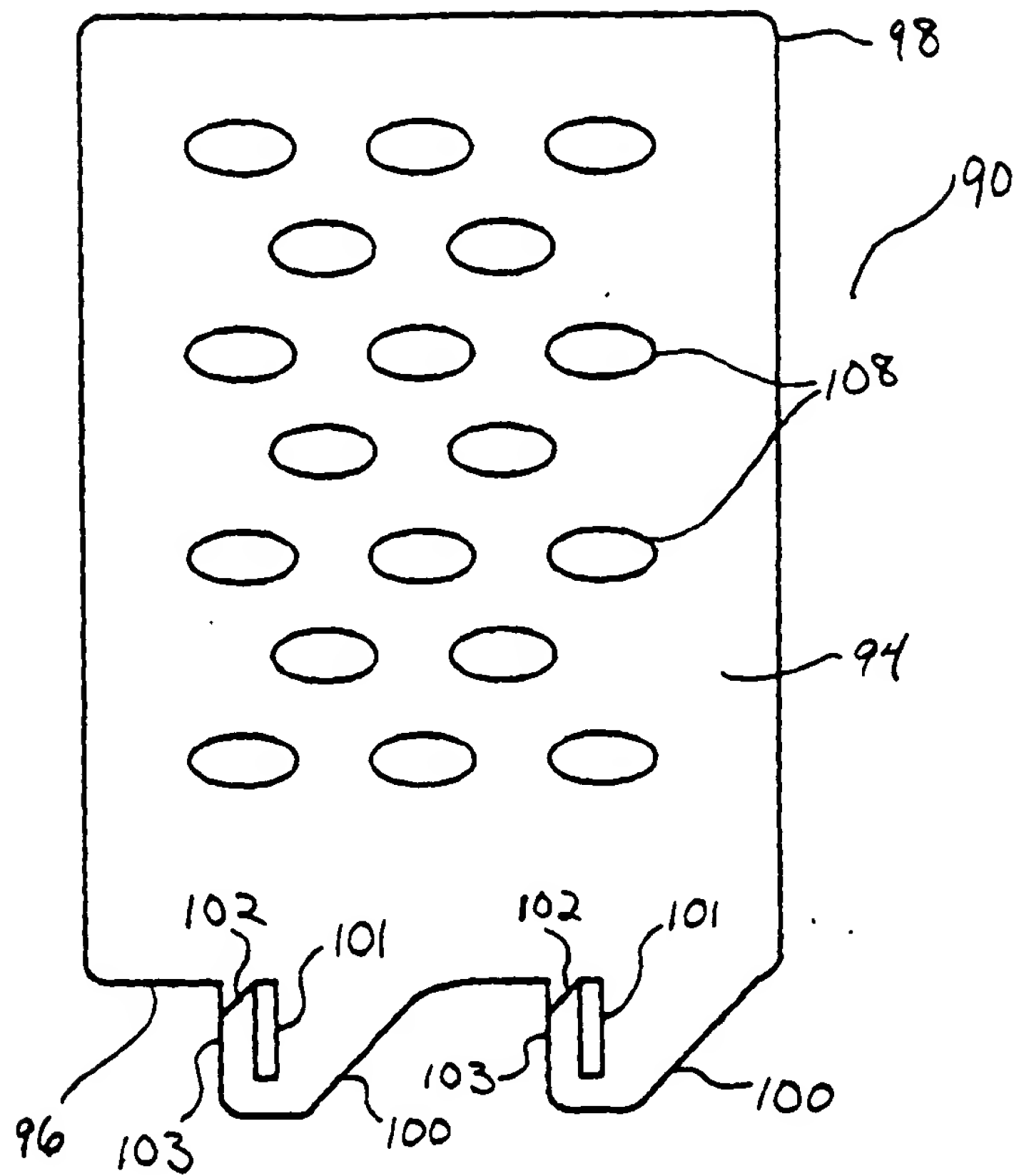


FIG. 14

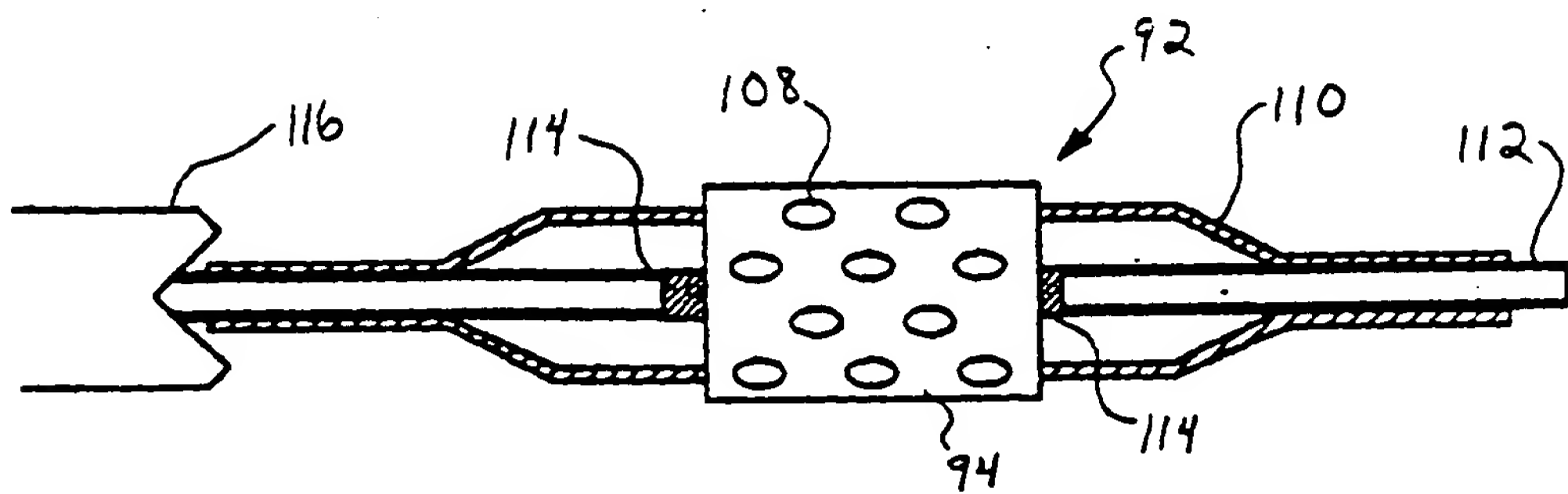


FIG. 15

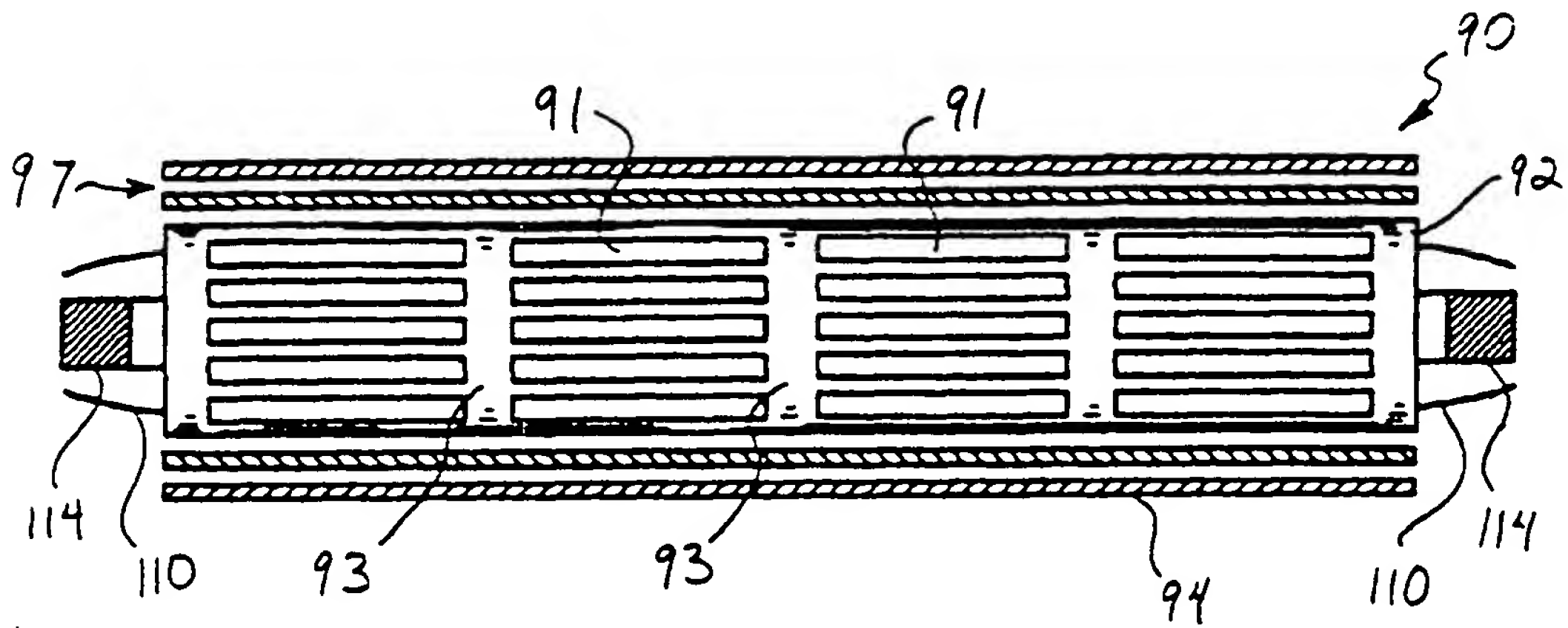


FIG. 16

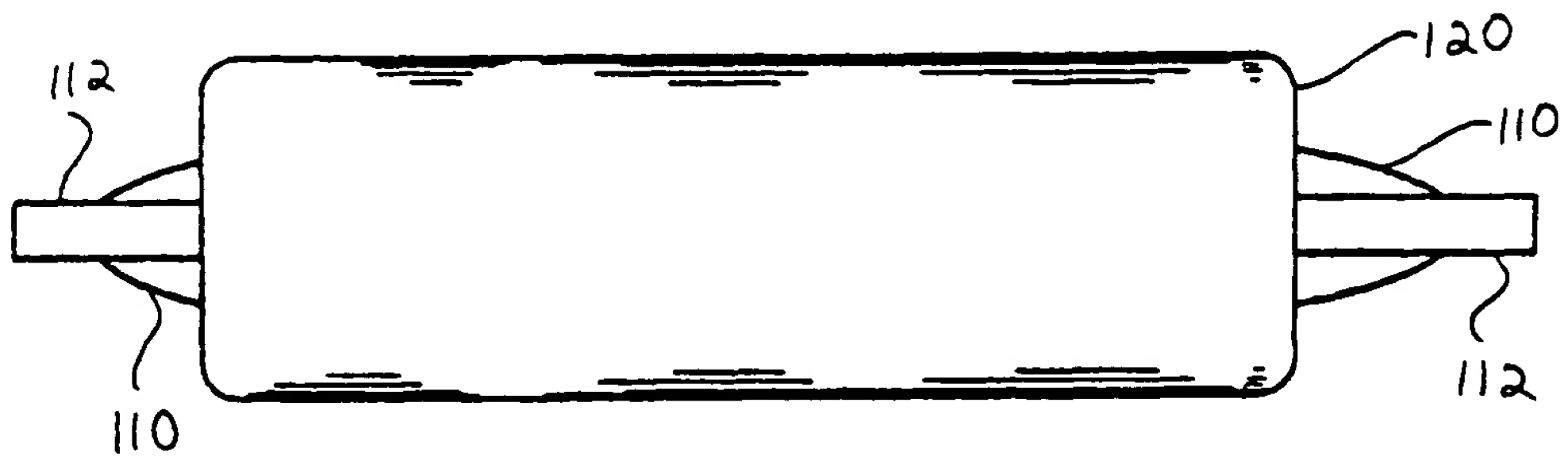


FIG. 17

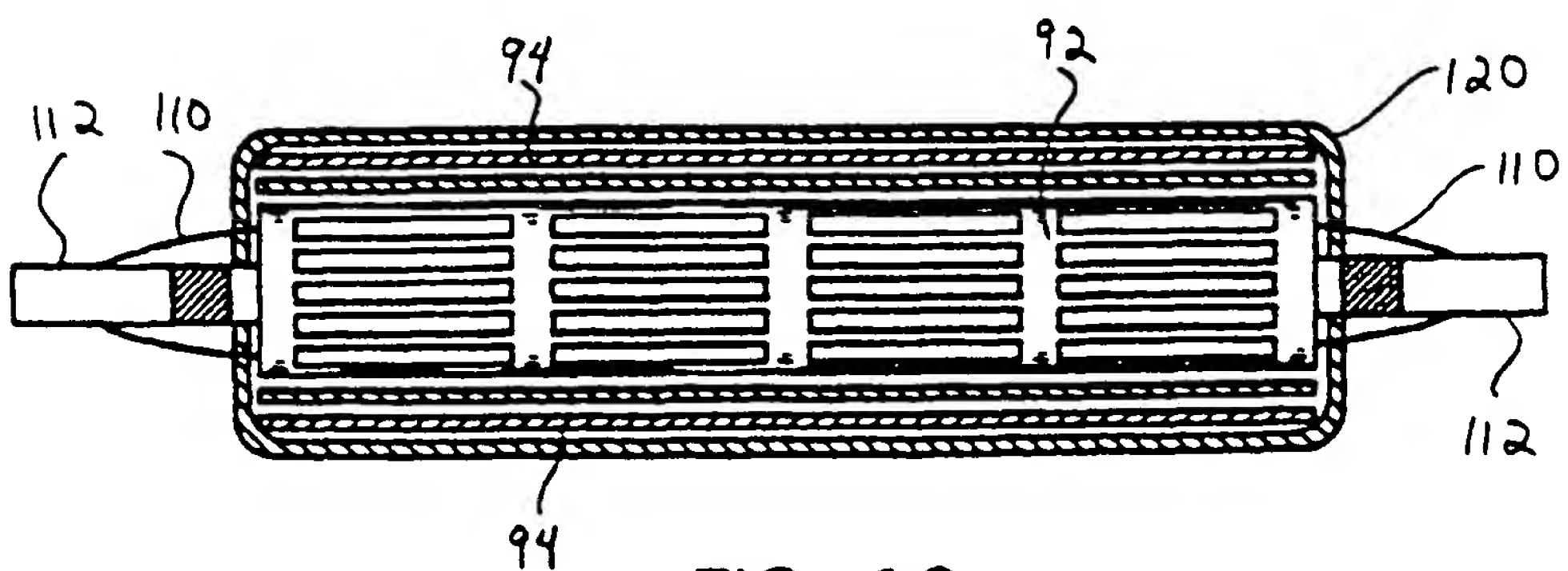


FIG. 18